Response to Office Action Mailed: April 11, 2007 Response Electronically Filed October 5, 2007

Amendments to the Specification

(1) Please add the following after Page 62, line 5, of the specification:

Brief Description of the Drawings

Figure. 1 shows the recovery of relative activity (penetrant amount) in different layers of the skin as a function of applied activity (dose).

Figure 2 shows the amount of carrier derived radioactivity (³H-DPPC) in the blood as a function of time and epicutaneously administered penetrant quantity, expressed as percentage of applied dosage.

Figure 3 indicates the relative accumulation of carrier derived radioactivity in various organs at two different time points after an increasing mass of ultradeformable carriers has been administered on the skin.

Figure 4 shows the absolute penetrant distribution profile (in arbitrary units) in different layers of the skin as a function of applied activity (dose).

Figure 5 shows the total amount of penetrant recovered in different tissues (skin, blood, liver) at different times after the administration of an increasing quantity of ultradeformable penetrants on the skin.

Figure 6 shows the time dependence of penetrant derived radioactivity in the blood as a function of epicutaneously administered suspension volume (lipid amount).

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Figure 7 shows the penetrant derived radioactivity in the blood as a function of epicutaneously administered dose measured 8 h or 24 h after the application.

Figure 8 shows the results obtained by measurement of the mean vapour transmission rate (MVTR) of five microporous polyethylene membranes, four polyurethane membranes and one polycarbonate track etched membrane.

Figure 9 is a diagram showing the principle of the "switching-effect", which is observed in connection with the inventive hydrophobic mesh-membranes.

Figure 10 shows the penetrability of three different microporous polyethylene membranes to Transfersomes®.

Figure 11 shows a schematic diagram of a multicompartment patch having external compartments according to the present invention in form of a twin syringe serving as storage compartments with mixing tubing or a T-piece connector attached to the patch.

Figure 12 shows a schematic diagram of a multicompartment patch according to the present invention having vertically stacked compartments.

Figure 13 shows a schematic diagram of a multicompartment patch according to the present invention with a side-by-side alignment of compartments with vertically introduced septum.

Figure 14 shows a schematic diagram of a multicompartment patch according to the present invention having a side-by-side alignment of compartments with separating lamination.

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Amendments to the Specification (cont.)

(2) Please replace the paragraph at page 31, line 28 to page 32, line 5 with the following:

Said backing liner <u>needs</u> need to be liquid-tight in order to prevent loss of active substance, which should be delivered e.g. transdermally. In order to ensure or determine if the membrane is liquid-tight, the penetrability of Transfersomes® through the membranes is measured upon application of low hydrostatic pressures. The polyethylene membranes Cotran 9711 (3M Medica, Borken Germany) and 14P10A are liquid tight up to an applied pressure of 1 MPa. Further, all cited polyurethane membranes are liquid tight.

Non-Marked-Up Version of Amendment to Specification:

Below is presented amendment (1) with the text to be added after Page 62, line 5, of the

specification, without any underlining, as required by 37 C.F.R. § 1.121(b)(1)(iii):

Brief Description of the Drawings

Figure 1 shows the recovery of relative activity (penetrant amount) in different layers of the

skin as a function of applied activity (dose).

Figure 2 shows the amount of carrier derived radioactivity (³H-DPPC) in the blood as a

function of time and epicutaneously administered penetrant quantity, expressed as percentage

of applied dosage.

Figure 3 indicates the relative accumulation of carrier derived radioactivity in various organs at

two different time points after an increasing mass of ultradeformable carriers has been

administered on the skin.

Figure 4 shows the absolute penetrant distribution profile (in arbitrary units) in different layers

of the skin as a function of applied activity (dose).

Figure 5 shows the total amount of penetrant recovered in different tissues (skin, blood, liver)

at different times after the administration of an increasing quantity of ultradeformable

penetrants on the skin.

Figure 6 shows the time dependence of penetrant derived radioactivity in the blood as a

function of epicutaneously administered suspension volume (lipid amount).

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Figure 7 shows the penetrant derived radioactivity in the blood as a function of epicutaneously

administered dose measured 8 h or 24 h after the application.

Figure 8 shows the results obtained by measurement of the mean vapour transmission rate

(MVTR) of five microporous polyethylene membranes, four polyurethane membranes and one

polycarbonate track etched membrane.

Figure 9 is a diagram showing the principle of the "switching-effect", which is observed in

connection with the inventive hydrophobic mesh-membranes.

Figure 10 shows the penetrability of three different microporous polyethylene membranes to

Transfersomes®.

Figure 11 shows a schematic diagram of a multicompartment patch having external

compartments according to the present invention in form of a twin syringe serving as storage

compartments with mixing tubing or a T-piece connector attached to the patch.

Figure 12 shows a schematic diagram of a multicompartment patch according to the present

invention having vertically stacked compartments.

Figure 13 shows a schematic diagram of a multicompartment patch according to the present

invention with a side-by-side alignment of compartments with vertically introduced septum.

Figure 14 shows a schematic diagram of a multicompartment patch according to the present

invention having a side-by-side alignment of compartments with separating lamination.

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Non-Marked-Up Version of Amendment to Specification (cont.):

Below is presented amendment (2) with the text of the replacement paragraph for the paragraph from page 31, line 28, to page 32, line 5, without any underlining, as required by 37 C.F.R. § 1.121(b)(1)(iii):

Said backing liner needs to be liquid-tight in order to prevent loss of active substance, which should be delivered e.g. transdermally. In order to ensure or determine if the membrane is liquid-tight, the penetrability of Transfersomes® through the membranes is measured upon application of low hydrostatic pressures. The polyethylene membranes Cotran 9711 (3M Medica, Borken Germany) and 14P10A are liquid tight up to an applied pressure of 1 MPa. Further, all cited polyurethane membranes are liquid tight.